Effect of Right Ventricular Versus Biventricular Pacing on Electrical Remodeling in the Normal Heart

Samir Saba, MD; Haider Mehdi, PhD; Michael A. Mathier, MD; M. Zahadul Islam, MBBS; Guy Salama, PhD; Barry London, MD, PhD

**Background**—Biventricular (BIV) pacing can improve cardiac function in heart failure by altering the mechanical and electric substrates. We investigated the effect of BIV versus right ventricular (RV) pacing on the normal heart.

**Methods and Results**—Male New Zealand White rabbits (n=33) were divided into 3 groups: sham-operated (control), RV pacing, and BIV pacing groups. Four weeks after surgery, the native QT (P=0.004) interval was significantly shorter in the BIV group compared with the RV or sham-operated groups. Also, compared with rabbits in the RV group, rabbits in the BIV group had shorter RV effective refractory period at all cycle lengths and shorter LV paced QT interval during the drive train of stimuli and close to refractoriness (P<0.001 for all comparisons). Protein expression of the KVLQT1 was significantly increased in the BIV group compared with the RV and control groups, whereas protein expression of SCN5A and connexin 43 was significantly decreased in the RV compared with the other study groups. Erg protein expression was significantly increased in both pacing groups compared with the controls.

**Conclusions**—In this rabbit model, we demonstrate a direct effect of BIV but not RV pacing on shortening the native QT interval as well as the paced QT interval during burst pacing and close to the ventricular effective refractory period. These findings underscore the fact that the effect of BIV pacing is partially mediated through direct electric remodeling and may have implications as to the effect of BIV pacing on arrhythmia incidence and burden. *(Circ Arrhythm Electrophysiol. 2010;3:79-87.)*

**Key Words:** rabbit ▪ right ventricular pacing ▪ biventricular pacing ▪ cardiac remodeling

Both mechanical and electric reverse remodeling have been documented with biventricular pacing (BIV) in patients with advanced heart failure (HF) and systolic left ventricular (LV) dysfunction.1–3 Other interventions that have significant salutary effects from the hemodynamic perspective, such as the insertion of LV assist devices, have also been shown to alter the electric characteristics of the failing heart, as demonstrated by the surface ECG.4 It is unclear, however, whether these electric changes are a consequence of the reverse mechanical remodeling or whether they are a direct effect of the site of pacing and altered electric and mechanical propagation.

**Clinical Perspective on p 87**

We have previously demonstrated in a novel rabbit model of myocardial infarction and chronic epicardial pacing that unlike right ventricular (RV) pacing or no pacing, BIV pacing reduces both LV end-systolic and end-diastolic volumes, increases the LV fractional area shortening, and restore the ether-a-gogo myocardial protein levels to their preinfarction levels. BIV pacing also shortens the native QRS complex in rabbits 4 weeks after myocardial infarction.5 Whether these electric changes are secondary to the mechanical improvement in LV size and function or whether they are independent of these changes and possibly upstream of them from the mechanistic standpoint remains unclear at this point.

The effect of pacing on altering the T-wave vector of the normal heart in sinus rhythm has been termed “cardiac memory” and is well described in the literature.6,7 Human reports and animal models have described this phenomenon in the context of RV pacing, anomalous ventricular preexcitation, or arrhythmias. To our knowledge, the differential effect of RV versus BIV pacing on cardiac electric remodeling in the normal heart has not been described in the literature.

We therefore investigated the effect of BIV versus RV pacing on the normal heart, where significant changes in mechanical function are not expected, to elucidate which changes induced with BIV pacing may be a direct consequence of the altered electric stimulation.

**Materials and Methods**

**Study Design**

The research protocol was approved by the Institutional Animal Care and Use Committee of the University of Pittsburgh. Male New...
Zealand white rabbits (n = 33; weight, 3.4 to 6.0 kg) were divided into 3 groups: sham-operated controls (C group, n = 9), in which the rabbits underwent pericardial stripping only; RV pacing group (RV group, n = 11), in which the rabbits underwent pericardial stripping and epicardial RV pacemaker implantation; and BIV pacing group (BIV group, n = 13), in which the rabbits underwent pericardial stripping and epicardial BIV pacemaker implantation. All paced rabbits (RV and BIV groups) had both RV and LV epicardial leads. Rabbits in the pacing groups were continuously paced at a rate of 270 beats per minute, which is slightly higher than the maximum ambulatory heart rate in the rabbit, for 4 weeks after surgery until they were euthanized. Rabbits had baseline ECGs and echocardiograms on the day of surgery. At 4 weeks, rabbits had a repeat ECG and echocardiogram done after the pacemaker was turned off for no less than 30 minutes. A total of 8 rabbits (4 in each of the RV and BIV groups) underwent programmed ventricular stimulation 4 weeks after surgery. They were then euthanized and their hearts were excised. Cardiac tissue was collected from the LV and RV of all 3 groups for molecular analyses.

Surgical Preparation of Rabbit
As previously described,5,8 rabbits were anesthetized using intramuscular injections of a mixture of ketamine (35 mg/kg) and xylazine (5 mg/kg). A 22-gauge intravenous catheter was inserted into the marginal ear vein for venous access. An arterial line was inserted into the middle ear artery for continuous hemodynamic monitoring. The rabbits were intubated with an endotracheal tube (3.0-mm inner diameter) and mechanically ventilated (rate, 40/min; tidal volume, 15 mL) using room air enriched with oxygen. Isoflurane anesthesia (2.0% to 2.5%) was delivered to maintain general anesthesia during surgery. The rabbits were placed on a water blanket adjusted to 38°C. A pulse oximeter was placed on the rabbit’s tongue for continuous monitoring of oxygen saturation.

The chest was opened through the fourth left intercostal space. The heart was exposed through an incision of the pericardium and explored. Prophylactic antibiotic (Ancef, 100 mg IV) was administered before and after surgery.

Pacemaker Implantation
As previously described,5,8 pacemaker leads were sutured to the epicardial surface of both the RV and the LV. The LV and RV leads were placed on the LV and RV free walls, respectively. The leads (model 4965 and model 4968, Medtronic, St Paul, MN) were connected to a permanent pacemaker configured to pace the RV alone or both the RV and LV simultaneously. In the case of BIV pacing, a Y-connector (model 2872, Medtronic) was used to pace the RV and LV simultaneously from a single-chamber (Kappa KSR403, Medtronic) pacemaker, programmed through research software to pace at a fast rate of 270 beats per minute (slightly above the rabbit’s maximum ambulatory heart rate within a cage) to ensure a high percentage of pacing. Before Y-adapting the RV and LV leads, they were both tested for sensing as well as pacing impedance and threshold, and the morphology of the captured QRS complex from each lead was noted. Once connected to the pacemaker, a QRS morphology consistent with a fusion between RV and LV pacing was ascertained to confirm capture of both ventricles. Pacing was ascertained by weekly interrogation of the pacemaker. The pacemaker and leads were placed in a subcutaneous pocket in the abdominal area of the rabbit.

Echocardiography
Nineteen rabbits (9 control, 6 RV, and 4 BIV) underwent baseline and follow-up echocardiography 4 weeks after surgery. As previously described,5,8 after anesthesia with ketamine and xylazine, rabbits were placed supine on a warming plate and the chest was shaved. Needle ECG leads were attached to each limb for continuous ECG monitoring. Echocardiography was performed with the pacemaker turned off, with an Acuson Sequoia ultrasound machine using a dynamically focused 8-MHz transducer. Two-dimensional long- and short-axis images through the LV were obtained and the latter used to place the M-mode cursor perpendicularly through the LV septum and posterior wall, avoiding the papillary muscles and imaging at the level of maximum chamber dimension. Studies were recorded on half-inch S-VHS videotape and freeze-frame images, including the ECG, printed on a color printer.

Off-line data analysis was performed on the echocardiographic images. LV cross-sectional areas at end-diastole (CSAd) and at end-systole (CSAs) were measured from freeze-frame 2D mode in the short-axis view by planimetry. End-diastole was taken to be at the point of maximal cavity dimension and end-systole at the point of maximal anterior excursion of the posterior wall. Three or more beats were measured and averaged. The LV percent fractional area change (%FAC) was calculated as (CSAd−CSAs)/CSAd×100. All echocardiograms were read in random order by an observer masked to the experimental group of the rabbits.

Ventricular Stimulation Protocol
Premature ventricular stimulation was performed on 8 rabbits (4 RV and 4 BIV) 4 weeks after surgery. Inhaled isoflurane (2.5%) was used during the protocol. The pacemaker was turned off for no less than 30 minutes before ventricular stimulation. After disconnecting them from the pacemaker and the Y-adapter, the RV and LV leads were used for stimulation. Single premature ventricular stimuli (S2) were delivered from the RV and LV leads after a drive of 12 ventricular stimuli (S1) at cycle lengths of 260, 240, 220, 200, 180, 160, and 140 ms, until the ventricular effective refractory period (VERP) was reached. The QRS and QT intervals were measured while pacing from the RV and LV at each cycle length, both during the pacing drive and immediately before reaching the VERP (at the functional refractory period).

Optical Mapping
Optical mapping was performed on a subset of 4 control rabbits to assess the duration of the action potential at 75% repolarization (APD75) in RV compared with LV tissue. As previously described,8 hearts excised from rabbits were hung on a Langendorff apparatus and retrogradely perfused through the aorta. The hearts were stained with the voltage dye RH-237, and action potential transients were recorded at 37°C from the epicardial surface of the LV and RV. The optical mapping array consists of 16×16 diodes, with each diode having a sensing area of 0.95×0.95 mm², with a pitch of 1.1 mm (center of one diode to adjacent diode). Diodes at the 4 corners of the array are used as instrumentation data channels, resulting in 252 of 256 diodes being monitored for voltage signals. Each diode detects light from an area of 0.8×0.8 mm² from the epicardial layer. Various regions of the heart were scanned including in the LV and RV. The mean APD75 was calculated for each ventricle in the 4 control rabbits.

Cellular and Molecular Analysis of Cardiac Tissue
Hearts were removed from rabbits in each experimental group, and 200-mg samples were taken from the LV and RV free walls. We performed immunoblots (Western blots) using antibodies to the ether-a-go-go-related gene (erg) (rabbit anti-erg [Kv11.1] polyclonal antibody from Chemicon International Inc, Temecula, Calif; KV-LQT1 from Alomone Labs, catalog No. APC-022, Jerusalem, Israel; Kv4.3 from Alomone Labs, catalog No. APC-017; SCN5A from Alomone Labs, catalog No. ASC-005; and connexin 43 from Mil- pore, catalog No. MBA3067, Temecula, Calif) genes. As previously described,5,9,10 crude membrane preparations were isolated by differential centrifugation from the same regions of the hearts described above. Channel proteins were dissolved in buffer containing SDS, quantitated (BioRad), and ~60 μg of protein per lane was run on a 7.5% SDS-PAGE gel (ready tris-HCL gel from Bio-Rad Laboratories, Hercules, Calif), transferred to PVDF membrane by semidry apparatus, blocked with PBS–5% milk, incubated overnight at 4°C with the primary antibody, washed with PBS-Tween, incubated with alkaline phosphatase (AP)-conjugated goat anti-mouse 2nd antibody, and quantified by chemiluminescence (Lumi-Phos). Coomassie Blue staining of SDS-PAGE gels was performed to confirm equal.
loading. The autoradiographs were scanned using a Visioneer One-Touch scanner (Visioneer Hardware, Pleasanton, Calif) and Micro-Scan and Camera Wizard computer program. The images were digitzed for quantification using Qucnty One quantitation software (BioRad). Bands of interest were delineated and densitometries were calculated based on the number of pixels. To allow comparison between blots, samples on each blot were normalized against the mean of the samples from the same ventricle and densitometries were calculated based on the number of pixels. The autoradiographs were scanned using a Visioneer One-Touch scanner and Camera Wizard computer program. The images were digitized for quantification using Quantity One quantitation software (BioRad). Bands of interest were delineated and densitometries were calculated based on the number of pixels. 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Results

Electrocardiography

ECGs were obtained on all 33 rabbits at baseline and 4 weeks after surgery. All ECGs were obtained while the pacemaker was turned off for no less than 30 minutes. The tracings were analyzed and the data are presented in Table 2.

At baseline, there were no differences between groups in any of the measured parameters. At 4 weeks after surgery, there were no significant differences in R-R, PR, or QRS intervals among the 3 study groups (Table 2). Four weeks after surgery, the QT interval was significantly shorter in the

Table 2. Electrocardiographic Data

<table>
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<th>RR, ms</th>
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<th>QRS, ms</th>
<th>QT, ms</th>
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<td>4w</td>
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<td>Control (n=9)</td>
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<td>324 (17)</td>
<td>76 (5)</td>
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<td>RV (n=11)</td>
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<td>295 (12)</td>
<td>76 (3)</td>
<td>87 (4)</td>
<td>44 (1)</td>
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<td>BIV (n=13)</td>
<td>313 (12)</td>
<td>298 (10)</td>
<td>76 (2)</td>
<td>78 (3)</td>
<td>41 (2)</td>
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All measurements are represented as mean (SE). QT index is the percentage of the ratio of the QT measured to the QT expected based on the heart rate. QT expected is calculated using the equation QT exp = 86 + 0.22 × R-R, where R-R is the cardiac cycle length. Base indicates baseline presurgery value; 4w, 4 weeks after surgery. *P<0.01 for the comparison of BIV group versus control and RV groups. †P<0.05 for the comparison of BIV group versus control and RV groups.
Figure 1. Mean ± SE of VERP (A), QT interval (B), and QT interval at the functional refractory period (C), pacing from the RV (left panel) and LV (right panel) at cycle lengths of 260 ms, 240 ms, 220 ms, 200 ms, 180 ms, 160 ms, and 140 ms, in both the RV (black) and BIV (gray) groups, after 4 weeks of pacing.
BIV group compared with the RV or sham-operated groups. Using established methods of correction of the QT interval in nontransgenic rabbits, the QT interval expected for the heart rate was calculated using the formula QT exp = 86 + 0.22 × R-R, where R-R represents the cardiac cycle length in milliseconds. The QT index, which is the percentage of the ratio of the measured to the expected QT, was then derived. As shown in Table 2, the QT index in the BIV group was significantly smaller than in the RV or control groups.

**Premature Ventricular Stimulation**

At baseline, there were no differences between the RV and BIV paced groups in any of the parameters including the ventricular refractory periods of the RV and LV as well as the QRS and QT intervals during drive pacing (S1) from the RV and LV as well as at the functional refractory period determined with premature ventricular stimulation (S2) at all cycle lengths. Four weeks after surgery, compared with rabbits in the RV group, rabbits in the BIV group had significantly shorter RVERP at all cycle lengths and shorter LV paced QT interval during the drive train of stimuli and at the functional refractory period during premature ventricular stimulation (Figure 1). Also, 4 weeks after surgery, the paced QRS width at the functional refractory period was marginally narrower in the RV compared with the BIV group during RV pacing (94 ± 1 ms versus 98 ± 1 ms, \( P = 0.025 \) for the overall comparison between study groups) and trended toward marginally wider in the RV compared with the BIV group during LV pacing (98 ± 2 ms versus 93 ± 2 ms, \( P = 0.056 \) for the overall comparison between study groups) at all cycle lengths. All other parameters were comparable between the RV and BIV groups. No rabbits in any of the study groups were inducible into sustained ventricular arrhythmias with premature ventricular stimulation.

**Action Potential Duration**

In 4 control rabbits, the APD75 was measured in the RV and LV tissue using optical mapping techniques. In the control rabbits, the mean APD75 duration was significantly longer in the RV compared with LV tissue (143 ± 36 ms versus 113 ± 15 ms, \( P = 0.001 \), Figure 2).

**Tissue Analysis**

Protein expression of the Kv4.3 gene was similar among the 3 study groups (data not shown). With pacing, the protein expression of the Erg gene in the LV and RV was significantly increased in the RV and BIV groups compared with the sham-operated controls, but there was no difference in expression of the Erg protein between the RV and BIV groups (Figure 3). With BIV pacing, the protein expression of the LV but not RV KVLQT1 gene was significantly increased compared with the RV pacing group and the control group, potentially accounting for the shorter repolarization time on surface ECG in the BIV group compared with the 2 other study groups (Figure 4). With BIV pacing, the protein expression of SCN5A in the LV was significantly increased compared with the RV pacing group and the control group, and the expression in the RV pacing group was significantly reduced compared with control group. The protein expression of RV SCN5A did not demonstrate significant differences among the study groups (Figure 5). Similarly, the protein expression of the LV but not RV connexin43 gene was significantly increased in the BIV pacing group compared with the RV pacing group (Figure 6).

Levels of mRNA for all 4 genes of interest (Erg, KVLQT1, SCN5A, and Connexin43) were not different among these 3 groups of rabbits (data not shown), suggesting a post-transcription mechanism for the differences seen in protein levels between the RV and BIV paced groups, possibly secondary to translation, protein trafficking, or degradation.

**Discussion**

In this study, we present data on the effect of BIV pacing on electric remodeling in the normal rabbit heart. Four weeks of BIV pacing resulted in significant shortening of the native measured QT interval on the surface ECG as well as a significantly smaller QT index, suggesting a direct effect of the sites of pacing on the repolarizing currents in the ventricular myocardium. This is further supported by the results of the ventricular premature stimulation protocols, which demonstrated shortening of the VERP as well as of the LV paced QT intervals at various cycle lengths with BIV versus RV pacing. The increased protein expression of both the KVLQT1 and erg genes provides a molecular correlate for the abbreviated repolarization time in the BIV rabbit hearts.

A possible mechanistic explanation for the findings during invasive electrophysiological testing is that RV as compared with BIV pacing further prolongs the local RV repolarization time beyond the baseline longer APD of RV compared with LV tissue, thus leading to longer RVERP in the former compared with the latter group. The lack of difference between the study groups in the QT interval during RV...
pacing is actually due to the early stimulation of the RV tissue with its longer repolarization time. During LV pacing, on the other hand, RV tissue is excited late and therefore its delayed repolarization contributes to the longer global QT interval. The demonstrated differences in the levels of SCN5A and connexin43 proteins mainly seen in LV tissue may also contribute to the shorter repolarization time in BIV compared with RV paced rabbits through mechanisms that may involve modification of the restitution of the sodium channel or alteration of the virtual electrode effect. These mechanisms are suggested by our findings but remain unproven.

A salutary effect of BIV pacing has been demonstrated in patients with heart failure with advanced cardiac structural abnormalities.1–3 In those patients, evidence of electric remodeling in the form of shortened QRS duration has been demonstrated in conjunction with improved myocardial function and patient symptoms.13 Whether the altered electric substrate is the result of improved hemodynamics or whether it is a direct effect of altered electric stimulation is not clear. Our data suggest that the electric remodeling is at least in part due to a direct effect of pacing, because in our rabbit model, there were no observed structural abnormalities of the heart, except for a minor decrease in fractional area shortening in the RV compared with the BIV paced rabbits, which cannot account for the differences in repolarization parameters documented between the BIV and control groups.

Cardiac repolarization changes after pacing, commonly referred to as “cardiac memory,” have been extensively described in the literature.6,7 This phenomenon describes a change in the T-wave vector in sinus rhythm on the surface ECG as a result of a preceding period of altered ventricular depolarization such as would happen during pacing or arrhythmia. The altered T-wave vector in sinus rhythm reflects the direction of depolarization during pacing or arrhythmia, as if the T wave remembers the direction of the QRS complex during that period, thus the term “cardiac memory.” The underlying mechanisms for cardiac memory have been studied at the cellular and molecular levels and shown to involve altered ion channel expression and function (mainly the transient outward current Ito) as well as altered myocardial gene expression.7 Short-term cardiac memory has been shown to induce uniform shortening of ventricular repolarization time by ~10 ms in open-chest dogs paced for 2 hours.14 Long-term cardiac memory has also been shown to induce T-wave changes after 3 weeks of pacing that are maximal close to the site of pacing.15 Put together, these results suggest an effect of pacing as well as its site on cardiac repolarization that is also shown by our present data. To our knowledge, however, there are no reports in the literature on the effects of BIV pacing on cardiac memory.

Whether the documented electric changes seen with BIV pacing in our model can be attributed to cardiac memory seems highly improbable. First, the changes seen with cardiac
memory involve mainly a change in the direction of the T-wave vector rather than a change in the QT interval or measured ventricular refractory periods, which are the main altered parameters in our current study. Second, rabbits in the control and RV groups did not exhibit the shortening of the native QT interval that was demonstrated in the BIV paced group, suggesting that this shortening was not driven by pacing per se but rather by the sites of pacing. Whether the

Figure 4. KvLQT1 protein blot from the LV (A) and the RV (C) tissues for the 3 rabbit study groups (control [C], RV, and BIV). KvLQT1 bands as well as Coomassie-stained bands used to normalize for the protein load are shown. Also, the KvLQT1 bands for the 3 study groups are from the same blot with identical exposure. B, KvLQT1-peptide block, where the blot was exposed to anti-KvLQT1+petide (1:3 ratio). D and E, Graphic representation of KvLQT1 protein levels from LV (D) and RV (E) tissues for the 3 study groups. Note the statistically significant increase in KvLQT1 levels in the BIV group compared with the combined RV paced and control groups in the LV but not RV extracted tissue.

Figure 5. SCN5A protein blot from the LV (A) and the RV (B) tissues for the 3 rabbit study groups (control [C], RV, and BIV). C and D, Graphic representation of SCN5A protein levels from LV (C) and RV (D) tissues for the 3 study groups. Note the statistically significant increase in SCN5A levels in the BIV paced group compared with the RV paced and control groups and the lower SCN5A levels in the RV paced group compared with the control group in the LV but not RV extracted tissue.
mechanisms involved in cardiac memory are relevant to our findings cannot be completely ruled out and deserves further investigation.

We had previously demonstrated that in a rabbit model of chronic myocardial infarction, BIV pacing, unlike RV pacing or no pacing, restores Erg protein levels almost back to the normal levels documented in noninfarcted rabbits but does not shorten repolarization time. In our current normal heart model, QT is shortened with BIV pacing but not RV pacing, presumably because of the combined effect of increased expression of both the KVLQT1 and Erg genes. Whether the scar areas present in infarcted hearts create regional delays in repolarization times that preclude the shortening of the QT interval with BIV pacing despite favorable changes in gene expression is possible but not proven.

The effect of BIV pacing on the burden of ventricular arrhythmias in the failing heart has been investigated with discrepant results. Some studies have suggested an anti-arrhythmic effect of BIV pacing whereas others have reported a proarrhythmic effect from BIV pacing, presumably due to pacing very close to the reentrant circuit in the LV, thus facilitating the induction of reentrant ventricular arrhythmias. Whether the shorter repolarization time documented in our rabbit model, albeit in a normal heart, constitutes one of the mechanisms of reduced ventricular arrhythmia burden with BIV pacing in patients with heart failure remains unclear but deserves further investigation.

Because of several inherent characteristics, the rabbit heart has been used for many years as a model for studying the pathophysiology of the human heart. The fact that the rabbit cardiac action potential is similar to that of humans and the underlying channels and currents are also homologous has made the rabbit a very attractive species for studying electrophysiological phenomena. Moreover, the rabbit’s size is large enough to accommodate the implantation of permanent pacemakers designed for humans but modified to pace at fast rates. For all these reasons, we chose to use the rabbit in our present study.

The present study has few limitations. First, in our model, pacing the RV was done epicardially, which is different from the endocardial pacing typically used in clinical practice. It is unclear whether this difference affects the extrapolation of our results to humans. Second, we have empirically paced the rabbits in the RV and BIV groups at a rate of 270 beats per minute to ensure near continuous ventricular pacing. At this rate, we cannot rule out with certainty the possibility of a component of tachycardia-induced cardiomyopathy in the paced groups compared with the controls. This is partially supported by the fact that in both the RV and LV groups we documented slightly larger end-systolic and end-diastolic cross sectional areas compared with the control rabbits. There were, however, no significant differences in these parameters between the RV and LV groups, thus excluding the possibility that the observed differences in electric remodeling between these 2 study groups are due to differences in myocardial mechanics.

In summary, we present a rabbit model of pacing in the normal heart and demonstrate a direct effect of BIV but not RV pacing on shortening the native QT interval on the surface ECG, shortening the LV paced QT interval during burst pacing at various cycle lengths as well as close to refractoriness, and increased expression of the KVLQT1 protein expression. These findings in a normal heart underscore the fact that the effect of BIV pacing is at least partially mediated through direct electric remodeling, independent of mechanical phenomena, and may have implications as to the effect of BIV pacing on the incidence and burden of arrhythmias in the failing heart.
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Disclosures
None.

References
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